



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification³ : A61L 15/06	A1	(11) International Publication Number: WO 86/ 00532 (43) International Publication Date: 30 January 1986 (30.01.86)
(21) International Application Number: PCT/US84/01068 (22) International Filing Date: 7 July 1984 (07.07.84) (71) Applicant (for all designated States except US): FLEX-CON COMPANY, INC. [US/US]; Wall Street, Spencer, MA 01582 (US). (72) Inventor; and (75) Inventor/Applicant (for US only) : ABBER, Herman [US/US]; 60 Brian Drive, Brockton, MA 02400 (US). (74) Agent: KERSEY, George, E.; P.O. Box 126, Annandale, NJ 08801 (US). (81) Designated States: AT (European patent), AU, BE (European patent), CH (European patent), DE (European patent), FR (European patent), GB (European patent), JP, LU (European patent), NL (European patent), SE (European patent), US.		Published <i>With international search report.</i>
(54) Title: SILICONE PRESSURE SENSITIVE ADHESIVE AND USES (57) Abstract Silicone based pressure sensitive adhesives. Adhesives must satisfy an array of specific performance requirements when used in conjunction with transdermal therapeutic devices. A pressure sensitive adhesive has been formulated having favorable adhesive, shear, liquid permeability and release characteristics. The adhesive is a crosslinked polymerization product of a methyl/phenyl siloxane gum, dimethyl siloxane gum and a polysiloxane resin. The resulting adhesive provided suitable adhesion to a variety of surfaces and particular utility as an adhesive between plastic film and human skin as in transdermal therapeutic devices.		

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AT	Austria	GA	Gabon	MR	Mauritania
AU	Australia	GB	United Kingdom	MW	Malawi
BB	Barbados	HU	Hungary	NL	Netherlands
BE	Belgium	IT	Italy	NO	Norway
BG	Bulgaria	JP	Japan	RO	Romania
BR	Brazil	KP	Democratic People's Republic of Korea	SD	Sudan
CF	Central African Republic	KR	Republic of Korea	SE	Sweden
CG	Congo	LI	Liechtenstein	SN	Senegal
CH	Switzerland	LK	Sri Lanka	SU	Soviet Union
CM	Cameroon	LU	Luxembourg	TD	Chad
DE	Germany, Federal Republic of	MC	Monaco	TG	Togo
DK	Denmark	MG	Madagascar	US	United States of America
FI	Finland	ML	Mali		
FR	France				

SILICONE PRESSURE SENSITIVE ADHESIVE AND USES

BACKGROUND OF THE INVENTION

This application is a continuation in part of patent application Serial No. 324,362 filed November 24, 1981.

5 1. Field of the Invention

The present invention relates to pressure sensitive adhesives which provide suitable adherence of objects to the human skin. The invention relates more particularly to silicone based pressure sensitive adhesives which are
10 of particular use in transdermal therapeutic devices for attachment to the human skin.

2. Description of the Prior Art

Pressure sensitive adhesives for use on human skin are used typically in bandages or other therapeutic
15 devices which must adhere to the skin for a prescribed period of time. Such devices are typically comprised of a plastic or cloth film layer coated with a pressure sensitive adhesive. The pressure sensitive adhesive is protected with a release substrate which is readily
20 peelable from the adhesive coating. The pressure sensitive adhesive for use in connection with such bandages or other therapeutic device must satisfy an array of specific physical characteristics. Importantly the release substrate must be easily peelable from the
25 adhesive coating and the adhesive must have sufficient cohesion to keep the bandage or therapeutic object in adhesive contact with the skin for a prescribed period of time. Also the adhesive must not cause skin inflammation and must be nontoxic.

30 Additionally a pressure sensitive adhesive as applied to a transdermal therapeutic device must meet other strict performance requirements. A transdermal device is a medicinal pouch which contains a liquid medicine or other drugs which must be absorbed gradually into the skin over



a fairly long period of time. These devices typically contain a semipermeable membrane and are advantageously used with drugs which are best absorbed into the human body gradually, such as nitroglycerine or other drugs

5 useful in treating cardiac impairment. Thus, the pressure sensitive adhesive which is coated onto the therapeutic device must not act as a barrier to interrupt the flow of a fluid from the device and into the human blood stream. Specifically, the pressure sensitive adhesive must be

10 permeable to the drug being used. Furthermore, since the therapeutic device must remain in close adhesive contact with the skin over a period of time typically at least up to 24 hours, the adhesive should keep essentially all of the contact surface of the therapeutic device in adhesive

15 contact with the patient's skin over this entire period. The pressure sensitive adhesive should also permit the therapeutic device to be peeled from the skin without causing discomfort and without leaving an adhesive residue on the skin which is not easily removeable.

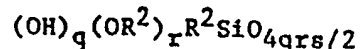
20 U.S. Patent Nos. 2,857,356 and 4,039,707 are illustrative of prior art silicone-based pressure sensitive adhesives. U.S. Patent No. 2,857,356 discloses a pressure sensitive adhesive formed from the polymerization of a silicate resin and an

25 organopolysiloxane fluid. The silicate resin is obtained by intercondensing a mixture comprising a cohydrolysis product of a trialkyl hydrolyzable silane and an alkyl silicate, said cohydrolysis product containing a plurality of silicone-bonded hydroxy groups. The formulation

30 disclosed in this reference is directed principally to forming a pressure sensitive adhesive which retains a high degree of tack and cohesion over a wide temperature range, for example between about -75°C and 250°C . The pressure sensitive adhesive product disclosed in this

reference is directed to application principally as an adhesive coating for use in contacting polymeric material such as glass, a wide range of plastics such as polyethylene, and also for use in connection with the manufacture of pressure sensitive tapes. There is no reference made in this disclosure to suitability of the adhesive product for application to human skin. In order to achieve the high degree of tack and cohesive strength, patentees disclose that the weight ratio of the silicate resin to the organopolysiloxane fluid should be between about 0.5/1 to 6/1, more preferably between about 1/1 to 3/1. (Column 7, lines 21 to 28). The range of formulations disclosed in this reference could not be suitable for application to a transdermal therapeutic device because of insufficient tack for application to human skin and too great a time lapse required to achieve maximum bonding.

U.S. Patent No. 4,039,707 discloses a siloxane-type pressure sensitive adhesive which is composed of the intercondensation product of a mixture containing an organopolysiloxane resin and at least one alkylaryl polysiloxane gum. The organopolysiloxane resin is defined at Column 6, lines 5 to 10 as having the formula:



It is also disclosed as essential that the organopolysiloxane gum contain aryl groups, such as phenyl groups, to obtain optimum pressure sensitive adhesive properties. If a mixture of phenyl and methyl groups is employed, this reference teaches that the number of silicone-bonded phenyl groups should be maintained with such a range that for each 2 to 75 phenyl groups attached directly to silicone by a carbon silicone linkage there are present from 98 to 25 silicone-bonded methyl groups, with the preferred range for instance from about 5 to 15

phenyl groups per 95 to 85 methyl groups. (Column 5, line 59 to Column 6, line 2). This reference also discloses a use of a release substrate covering the pressure sensitive adhesive. The release substrate may typically be a paper or polymer film coated with a release coating such as a silanol-stopped dimethylpolysiloxane fluid. Another release coating which is disclosed in this reference is based on dimethylvinyl-stopped dimethyl polysiloxane fluid. Additionally, the reference discloses that the alkylaryl polysiloxane gum should have a viscosity from about 200,000 to 15 million centipoise at 25°C and contain an average from about 1.85 to 2.01 silicone-bonded alkyl and aryl radicals per silicone atom.

Although use of an alkylaryl polysiloxane gum with an organopolysiloxane resin is disclosed in this reference, the reference does not disclose or suggest use of specific combinations of alkylaryl polysiloxane gums to improve the product's adhesive, shear and liquid permeability characteristics so that the adhesive product may be used with transdermal therapeutic devices.

Accordingly, it is an object of the present invention to provide an improved pressure sensitive adhesive which has particular use as an adhesive for retaining a plastic film or therapeutic device in adhesive contact with the human skin and which adhesive is nontoxic and easily removeable from the skin.

An important object of the invention is to provide a pressure sensitive adhesive for particular use in transdermal therapeutic devices. A related object is to provide pressure sensitive adhesive which retains the therapeutic device in adhesive contact with the human skin over a prolonged period of time and does not interfere with the absorption of medicinal fluid from the transdermal device through the adhesive and into the skin.

SUMMARY OF THE INVENTION

The pressure sensitive adhesive of the invention has been formulated to satisfy an array of specific performance requirements so that the product has a particular suitability for use as a pressure sensitive adhesive for transdermal therapeutic devices which are applied in adhesive contact with the skin. The pressure sensitive adhesive formulation is composed of the combination of a methyl/phenyl siloxane preferably dimethyl diphenyl siloxane gum with a dimethyl siloxane gum and an organopolysiloxane resin. Preferably, the resin is composed of monofunctional and quadrafunctional siloxane units, designated hereinafter as an MQ resin. Applicants have found that such a formulation provides a polymerized pressure sensitive adhesive having the requisite array of performance characteristics for use in connection with transdermal therapeutic devices. A suitable catalyst such as a diaryl peroxide catalyst is advantageously included in the mixture to initiate polymerization between the siloxane gum and resin to form the pressure sensitive adhesive product. Alternatively, the catalyst may be omitted and the polymerization initiated by other means.

Although it is conventional wisdom that dimethyl diphenyl siloxane gum is incompatible with dimethyl siloxane gum, applicants have found that over a specified range in concentration of these components in the presence of an MQ resin, a pressure sensitive adhesive product can be formed. The resulting adhesive product has an array of specific performance characteristics which make the product particularly suitable for use as a pressure sensitive adhesive for transdermal therapeutic devices. The weight ratio of a dimethyl diphenyl siloxane

6

gum to dimethyl siloxane gum should preferably be in a range between 1/3 to 3/1. In the embodiment including a catalyst, a diaryl peroxide catalyst may be used comprising between about 0.1 to 2 percent by weight of the polymerized pressure sensitive adhesive product. A preferred catalyst of this type is composed of 2, 4, dichloro benzoyl peroxide containing a phlegmatic agent such as dibutylphthalate. The pressure sensitive adhesive formulation may additionally include polybutene resin in an amount of up to approximately 15 percent by weight of the polymerized adhesive product.

An alternative formulation for the polymerized adhesive product of the invention is composed of dimethyl diphenyl siloxane gum, an organopolysiloxane resin (preferably MQ resin), and a suitable catalyst such as a diaryl peroxide catalyst as above described. The catalyst typically should be between about 0.1 to 5 percent by weight of the adhesive product. Although this formulation produces an acceptable product for use in connection with a transdermal therapeutic device, the product exhibits somewhat less satisfactory release characteristics in removing the release substrate from the adhesive as compared with the preferred formulation containing both dimethyl/diphenyl siloxane gum and dimethyl siloxane gum.

The polymerized pressure sensitive adhesive product is preferably prepared by forming a raw adhesive solution composed of the reactants set forth above, and solvents such as toluene, naphtha, xylene and n-butyl acetate. In the alternative formulations polybutene resin may be included, or as above-mentioned, the dimethyl siloxane gum may be omitted from the preferred formulation. The raw adhesive solution is prepared by mixing the siloxane gum, MQ resin, catalyst and solvents until a homogeneous solution is formed. The solution is coated onto a release



7

substrate (typically a paper sheet overcoated with a silicone release coating), thus forming an adhesive laminate. The adhesive laminate is dried to vaporize the solvents after which the laminate is heated to

- 5 temperatures necessary to initiate a polymerization reaction between the siloxane gum and MQ resin.

- The adhesive laminate may be transferred to a surface of a transdermal device so that the adhesive coating comes into direct contact with the device. Preferably, the
- 10 adhesive coating comes into direct contact with a semipermeable membrane component of the transdermal device. The user need only peel off the release substrate to expose the adhesive layer prior to pressing the transdermal device onto his skin. It has been found that
- 15 the pressure sensitive adhesive formulation of the invention exhibits unique liquid permeability characteristics and a high degree of adhesion to human skin, yet causes negligible skin irritation or redness and has excellent release properties permitting easy removal
- 20 of a release substrate from the adhesive.

DETAILED DESCRIPTION

The pressure sensitive adhesive of the invention is preferably composed of the combination of a methyl/phenyl siloxane gum; a dimethyl siloxane gum; an

- 5 organopolysiloxane resin, advantageously MQ resin; and suitable catalyst. A suitable methyl/phenyl siloxane gum is a dimethyl diphenyl siloxane. The term "gum" as used herein denotes a high viscosity, e.g. greater than about 20,000 centipoise, linear alkyl/aryl polysiloxane or
- 10 polydiorganosiloxane that can be converted from a highly viscous plastic state into the predominantly elastic state by crosslinking. See, W. Noll, "Chemistry and Technology of Silicones", Academic Press, New York (1958), p. 387. The term "organosiloxane elastomer" is hereinafter defined
- 15 as synonymous and interchangeable with the term "gum" as above-defined. See. W. Noll, *supra*, p. 387. The term "resin" as used in this patent application is synonymous with "polymer". The pressure sensitive adhesive is particularly useful for attaching a transdermal
- 20 therapeutic device to human skin for a period of up to about 24 hours. The adhesive exhibits favorable peel release characteristics and a high degree of adhesion over a prolonged period. The adhesive is particularly suited to medical applications in that it is easily removed from
- 25 the skin and nonirritating, and permits the medication in the transdermal device to pass from the device, through the adhesive, and thence into the skin.

- Transdermal devices are well known in the art. They are composed of a semipermeable microporous membrane or
- 30 membranes for storing a supply of liquid medication and causing release of the medication therefrom at constant rate over a prolonged period of time. The transdermal device containing the liquid medication is applied

directly to the skin in the form of a bandage. The semipermeable membrane in contact with the skin must be provided with a pressure sensitive adhesive layer in order to adhere to the skin. The references U.S. Patent Nos. 5 4,200,093 and 4,201,211 are merely representative of transdermal therapeutic devices to which the adhesive of the invention is applicable. The adhesive of the invention has general applicability to essentially any transdermal device which must be adhesively placed in 10 contact with the skin, and therefore the invention is not intended to be limited to the foregoing references but rather is incorporated by references herein merely for illustrative purposes.

A suitable adhesive for transdermal therapeutic 15 devices should satisfy a number of specific requirements. The adhesive must allow the liquid medicine to flow uninterrupted over a prolonged period of time, e.g. up to at least 6 hours and preferably up to at least 24 to 36 hours and longer, at constant rate, through the 20 semipermeable membrane and into the skin. Therefore, the adhesive cannot form a barrier between the membrane and the skin during the required prolonged period of use so as to measurably retard the constant rate of flow of the medicine from the membrane into the human skin. It has 25 been found that the adhesive formulation of the invention satisfies all the aforesaid requirements, whereas conventional pressure sensitive adhesives have been found to significantly retard the free flow of liquids therethrough, especially over a prolonged period.

30 Additionally, the adhesive should not cause undue irritation to the skin, including swelling, redness or itching on prolonged contact (typically up to at least 24 hours). The adhesive should also allow for relatively



easy removal of the transdermal device from the skin without causing great discomfort to the patient. In order to provide a suitable adhesive for use with a transdermal device, the adhesive should not significantly deteriorate
5 in strength or tend to peel or loosen over the 24 hour period. Additionally, there should be very little or no adhesive residue remaining on the skin after the transdermal device is peeled from the skin.

A pressure sensitive adhesive formulation which has
10 been found to satisfy the above requirements is presented as formulation A in Table I. The pressure sensitive adhesive formulation A is composed of a raw adhesive solution which is dried to evaporate the solvents and then cured to form the polymerized pressure sensitive adhesive
15 product A, having a composition shown in Table I.

Raw adhesive solution A as shown in Table I is composed of a methyl/phenyl siloxane gum such as dimethyl diphenyl siloxane gum, and organopolysiloxane resin, preferably MQ resin, dimethyl siloxane gum, suitable
20 catalysts and solvents. The methyl/phenyl siloxane gum such as dimethyl diphenyl siloxane gum as well as the dimethyl siloxane gum may typically have a viscosity between about 20,000 and 10,000,000 centipoise at 25°C, preferably between about 20,000 and 1,000,000 centipoise
25 at 25°C. The MQ resin included in formulation A is composed of monofunctional and quadrofunctional siloxane units and has the generic chemical formula: M_xQ_y , where $M = R_3SiO_{1/2}$; $Q = SiO_{4/2}$; and R preferably is a methyl group. However, R may include any other alkyl
30 group particularly C_1 to C_4 alkyl groups, i.e. methyl, ethyl, propyl and butyl alkyl groups.

The molar ratio of phenyl groups to methyl groups in the dimethyl diphenyl siloxane gum is at least about 0.1/1



- and preferably between about 0.1/1 and 0.2/1. Mixtures of dimethyl diphenyl siloxane gum and suitable MQ resin may be purchased under the tradename SILGRIP SR6574 manufactured by the General Electric Company of Waterford, New York. The MQ resin is commercially available in dry powdery particulate form. A preferred MQ resin to be added to this mixture is commercially available under the tradename CR542 from General Electric Company. Another MQ resin suitable for use in adhesive solution A is commercially sold under the tradename C42-2109 designated as a controlled release additive from Dow Corning Co. of Midland, Michigan. A suitable mixture of dimethyl siloxane gum and MQ resin is available under the trade designation 280 A adhesive from Dow Corning Co.
- The preferred catalyst is a diaryl peroxide type catalyst, such as that containing 2, 4, dichloro benzoyl peroxide, which contains a phlegmatic agent such as dibutyl phthalate. A catalyst of this type is available under the tradename CADOX TDP, available from Noury Chemical Company of Burt, New York. The raw adhesive solution A as set forth in Table I further contains solvents, preferably toluene, naphtha, xylene, and n-butyl acetate in the proportions listed.
- An alternate pressure sensitive adhesive formulation B is tabulated in Table II. This formulation has also been found to satisfy the above-referenced requirements. The pressure sensitive adhesive formulation B is composed of a raw adhesive solution which is dried to evaporate the solvents contained therein and then cured to form the polymerized pressure sensitive adhesive product B having a composition shown in Table II.
- The composition of formulation B is similar to that of formulation A except that a small amount of polybutene

- resin was found to be desirable because it produced greater tack and somewhat better adhesion. A suitable polybutene resin is available under the tradename INDOPOL (medium molecular weight) available from Amoco Company of Chicago, Illinois. The MQ resin included in formulation B has the generic formula M_xQ_y where $M = R_3SiO_{1/2}$, $Q = SiO_{4/2}$; and R preferably is a methyl group. However, R may be composed of any other alkyl group, particularly C_1 to C_4 alkyl groups such as methyl, ethyl, propyl and butyl alkyl groups. The dimethyl diphenyl polysiloxane gum included in raw adhesive solution B preferably has a molar ratio of phenyl groups to methyl groups at least about 0.1/1 and preferably between about 0.1/1 to 0.2/1.
- 15 A preferred formulation containing both dimethyl diphenyl siloxane gum and MQ resin for use in adhesive solution B is SILGRIP SR6574, available from the General Electric Company. A preferred MQ resin to be added to adhesive solution B is available under the tradename CR542
- 20 from General Electric Company. Another MQ resin suitable for use in adhesive solution B is sold under the tradename C42-2109 from Dow Corning Co. A preferred formulation containing both dimethyl siloxane gum and MQ resin for use in adhesive solution B may be purchased under the
- 25 tradename 280 A adhesive from Dow Corning Company.
- A suitable catalyst for formulation B is a diaryl peroxide type catalyst, such as that containing 2, 4 dichloro benzoyl peroxide which contains a phlegmatic agent such as dibutyl phthalate. A catalyst of this type
- 30 may be purchased under the tradename CADOX TDP from Noury Chemical Company. The raw adhesive solution as set forth in Table II further contains solvents toluene, naphtha, xylene and n-butyl acetate in the proportions listed.

Although the preferred catalyst shown in Tables I and II is a diaryl peroxide, such as 2, 4, dichloro benzoyl peroxide, other catalysts may be employed. Other catalysts include, for example, diacyl peroxide; amino silanes; secondary or tertiary amines; or an organic titanate such as terabutyl titanate available under the tradename TYZOR TBT from DuPont Company of Wilmington, Delaware. Alternatively, the catalyst may be omitted and the polymerization reaction initiated by other means such as electron beam contact.

Although the solvents listed in Tables I and II are most desirable, other solvents may be used, such as, for example toluene, naphtha and esters such as ethyl acetate and butyl acetate.

Although dimethyl diphenyl polysiloxane gum is preferred any methyl/phenyl polysiloxane gum may be used. Preferably, the methyl/phenyl polysiloxane gum has a molar ratio of phenyl groups to methyl groups between about 0.1/1 and 0.2/1. When employing as a basic ingredient one of the gum/resin mixtures recited above, the polymerized pressure sensitive adhesive product advantageously includes between about 0.1 to 15 weight percent of additional MQ resin and between about 0.1 to 2.0 weight percent catalyst. Typically the weight ratio of methyl/phenyl siloxane gum to dimethyl siloxane gum is in a range between about 1/3 to about 3/1 although a weight ratio approaching 3/1 is preferred.

Either of the adhesive solutions A or B may be made by mixing the constituents listed in Table I in a conventional closed mixing vat until a homogeneous solution is achieved. Although the various components may be added in any order, it is advantageous to premix the catalyst and solvents followed by addition of the



remaining components. The homogeneous raw solution is then coated onto a release substrate, typically composed of a paper sheet overcoated with a release coating such as conventional silicone release fluids; e.g.

- 5 polydimethylvinyl siloxane fluid containing appropriate catalysts such as one containing a noble metal complex. The overcoated release substrate forms an adhesive laminate sheet which is then dried, typically in conventional convective driers operating between
- 10 approximately 100°F to 200°F, in order to evaporate the solvents contained in the raw adhesive coating. The dried adhesive laminate is then passed through a curing oven operating at a temperature level of between about 200°F to 350°F, wherein a crosslinking type
- 15 polymerization reaction occurs between the siloxane gums, the MQ resin, and the catalyst.

- The adhesive laminate sheet containing the cured pressure sensitive adhesive product may be transferred directly to a surface of the semipermeable membrane of a
- 20 transdermal therapeutic device. Transfer may be accomplished by passing the adhesive laminate sheet and the semipermeable membrane film through a conventional laminator. The adhesive coated semipermeable membrane may then be cut into desired shapes for use in manufacture of
 - 25 transdermal therapeutic devices. In use of the transdermal device, the patient will peel off the release substrate portion of the adhesive laminate sheet thus exposing the adhesive coated semipermeable membrane so that direct contact can be made between the adhesive
 - 30 coated semipermeable membrane and the human skin.

Various performance tests for the polymerized pressure sensitive adhesive product were made for formulations tabulated in Table I and II. The results of the performance tests are tabulated in Table III.

15

TABLE IPressure Sensitive Adhesive (P.S.A.) - Formulation A

Raw Adhesive Solution A

		<u>Comp., Wt.%</u>
5	Mixture of Dimethyl Diphenyl Siloxane Gum Plus MQ Resin (e.g. SILGRIP SR 6574)	36.9
	Additional MQ Resin (e.g. CR 542)	0.5
10	Mixture of Dimethyl Siloxane Gum Plus MQ Resin (e.g. 280 A Adhesive)	12.5
15	Catalyst (e.g. Diaryl Peroxide and Phlegmatic Agent as in CADOX TDP)	0.2
	Solvent 1 Toluene	15.4
20	Solvent 2 Naphtha	15.1
	Solvent 3 Xylene	8.3
	Solvent 4 n-Butyl Acetate	11.1
25		100.0

16

TABLE I (CONT.)Polymerized Pressure Sensitive Adhesive Product A

Raw Adhesive Solution A

		<u>Comp., Wt.%</u>
5	Mixture of Dimethyl Diphenyl Siloxane Gum Plus MQ Resin (e.g. SILGRIP SR 6574)	73.6
	Additional MQ Resin (e.g. CR 542)	1.1
10	Mixture of Dimethyl Siloxane Gum Plus MQ Resin (e.g. 280A Adhesive)	24.9
	Catalyst (e.g. CADOX TDP)	0.4
15		100.0

17

TABLE II

Pressure Sensitive Adhesive (P.S.A.) - Formulation B
Raw Adhesive Solution B

		<u>Comp., Wt.%</u>
5	Mixture of Dimethyl Diphenyl Siloxane Gum Plus MQ Resin (e.g. As in SILGRIP 6574)	34.9
	Additional MQ Resin (e.g. CR 542)	0.9
10	Mixture of Dimethyl Siloxane Gum Plus MQ Resin (e.g. 280A Adhesive)	12.6
	Catalyst (e.g. CADOX TDP)	0.2
15	Polybutene Resin (e.g. Indopol 300)	1.7
	Solvent 1 Toluene	14.8
	Solvent 2	14.2
20	Naphtha	
	Solvent 3 Xylene	8.3
	Solvent 4 n-Butyl Acetate	12.4
25		100.0



TABLE II (CONT.)Polymerized Pressure Sensitive Adhesive Product B

		<u>Comp., Wt. %</u>
5	Mixture of Dimethyl Diphenyl Siloxane	69.4
	Gum and MQ Resin (e.g. SILGRIP 6574)	
	Additional MQ Resin (e.g. CR 542)	1.8
10	Mixture of Dimethyl Siloxane Gum and	25.0
	MQ Resin (e.g. 280A Adhesive)	
	Catalyst (e.g. CADOX TDP)	0.4
15	Polybutene Resin	3.4
	(e.g. Indopol 300)	<u>100.0</u>

TABLE III
PERFORMANCE TEST RESULTS

I. TEST SAMPLE FORMULATIONS	Adhesive		For Use With	
	Formulation A	Formulation B	Transdermal Thera- peutic Devices	
Adhesive Thickness	1.3 mil	2.2 mil	0.7	
Range	1.0 to 1.7 mil	1.3 to 3.2 mil	0.75 to 4.0	
II. PERFORMANCE				19
Degree of adhesion after 24 hours ¹	95 percent	95 percent	90 percent	
Peel adhesion from stainless steel (grams per inch width) ²	850	990	570	
Peel adhesion from release substrate (gms. per inch width) ³	120	50	20	

1. The percent of initial adhesive contact area remaining in contact with the skin.
2. Performed using Pressure Sensitive Tape Council Standard Test No. PSTC-1.
3. Measured with angle between the release substrate and the semipermeable membrane of ethylene vinyl acetate held at 90°.

TABLE III (CONTINUED)

PERFORMANCE TEST RESULTS

TEST SAMPLE FORMULATIONS	Dry Pressure Sens. Adhesive Formulation A	Dry Pressure Sens. Adhesive Formulation B	Minimum Required For Use With Transdermal Therapeutic Devices
Adhesive residue remaining 24 hours after removal of transdermal device from skin ⁴	5 to 10 percent	5 to 10 percent	Less than 20
Erythema (Irritation to skin) 6 hours	Almost imperceptible redness	Almost imperceptible redness	Barely perceptible redness
24 hours	None	None	Less than perceptible
Edema (Swelling or redness)			
6 hours	Negligible	Negligible	Negligible
24 hours	Less than 50 percent of occluded area	Less than 50 percent of occluded area	Less than 50 percent of occluded area
Itching	Mild	Mild	Mild
Permeability to Liquid (nitroglycerin release rate: mg/hr./cm ²) ₅	35 to 40	35 to 40	At least 30

4. Percent of initial adhesive contact area.

5. Average rate over a period of 27 hours using adhesive of thickness 2.2 ± 0.9

The production of a pressure sensitive adhesive in accordance with the invention is further illustrated by the following nonlimiting example:

EXAMPLE

- 5 A batch of raw adhesive solution was prepared in accordance with either of the formulations of Tables I and II. The catalyst was dispersed first into the solvents and the solvents with dispersed catalyst therein were then added to the siloxane gum and MQ resin constituents.
- 10 Dispersing the catalyst first in the solvents reduced the mixing time required to achieve a homogeneous solution. After the raw adhesive solution had been formed in accordance with the formulation shown in Table I the solution was mixed within a closed sealed drum with a high
- 15 speed air driven agitating mixer.

- The mixing was continued under ambient conditions until a homogeneous raw adhesive solution was obtained. The raw adhesive solution was then coated onto a release substrate which was composed of a paper sheet precoated
- 20 with a polydimethylvinyl siloxane fluid with the noble metal complex catalyst 7048 of Dow Corning Co. The raw adhesive was coated onto the release substrate using conventional three roll reverse rollers to achieve a coating thickness of about 3.5 mils. The release
- 25 substrate coated with the raw adhesive solution formed an adhesive laminate sheet.

- The adhesive laminate sheet was then passed through a conventional convective coater drier, operated under four temperature zones. The first zone included temperatures
- 30 between about 80° to 125°F; the second zone between about 125° to 200°F; the third zone between about 200° to 250°F and the fourth zone at about 350°F.



The adhesive laminate sheet passed continuously through the convective drier at about 40 feet per minute. The total length of the four zones was about 100 feet. As the adhesive laminate passed through the first two zones of the convective oven, the solvents evaporated from the raw adhesive solution which was coated onto the release substrate. Then as the adhesive laminate continued through zones 3 and 4, i.e., the curing zones, cross-linking polymerization reaction occurred forming the polymerized pressure sensitive adhesive product.

The adhesive laminate sheet containing the polymerized pressure sensitive adhesive coating was transferred onto a surface of a semipermeable membrane for use within a transdermal therapeutic device of which U.S. Patent Nos. 4,200,098 and 4,201,211 are merely illustrative. A conventional laminator was used to transfer the adhesive laminate onto the surface of the semipermeable membrane. The semipermeable membrane sheet with the attached adhesive laminate was then cut in predesignated shapes or stored in rolls for use in connection with the manufacture of transdermal therapeutic devices.

It will be appreciated that other formulations for the pressure sensitive adhesive product may be prepared in a manner similar to that set forth above without departing from the spirit and scope of the invention.



1 WHAT IS CLAIMED IS:

1. An adhesive that is permeable to medicinal fluids comprising the polymerization product of aryl polysiloxane, an alkyl polysiloxane and an MQ polysiloxane with multifunctional siloxane units.

2. The method of administering medicinal fluids which comprises the steps of

10 (a) placing a polysiloxane adhesive in contact with an epidermal layer;

(b) applying a polyfunctional derivative of a polyfunctional alcohol to said adhesive which is permeable thereto; thereby to permit said derivative to pass through said adhesive at a prescribed rate.

3. The method of preparing an adhesive for the transdermal passage of medicinal substances, which comprises

(a) providing an aryl polysiloxane;

(b) providing an alkyl polysiloxane;

20 (c) providing an MQ organopolysiloxane with multifunctional siloxane units; and

(d) polymerizing the mixture of said aryl polysiloxane, said alkyl polysiloxane and said MQ polysiloxane.

4. A combination of a medical device to be placed in adhesive contact with the skin and a pressure sensitive adhesive at least partially coated on said device, the adhesive permitting passage of medicinal liquids therethrough, said adhesive comprising:

30 the polymerization product of a mixture of reactants comprised of a linear methyl/phenyl polysiloxane gum, a linear dimethyl polysiloxane gum, and an MQ organopolysiloxane comprising monofunctional and quadrifunctional siloxane units,

35 the adhesive permitting passage of nitroglycerin therethrough at substantially constant rate of at least 30 mg./hr./cm² as measured over a 27-hour period with the adhesive having a thickness of about 2.2 ± 0.9 mil.



5. The combination of claim 1 wherein the medical device comprises a transdermal applicator for medicinal fluids.

6. The combination of claim 5 wherein the transdermal applicator comprises a semipermeable membrane.

7. The combination of claim 6 wherein the adhesive adheres to at least a portion of said semipermeable membrane.

8. A combination as in claim 1 wherein the adhesive has a thickness of at least 0.7 mil and permits at least 90 percent of the adhesive surface of the transdermal device in contact with the skin to remain adhesive after 24 hours..

9. A combination as in claim 1 wherein the adhesive has a peel adhesion from stainless steel of at least 570 gm. per inch width.

10. A combination as in claim 1 wherein the weight ratio of methyl/phenyl polysiloxane to dimethylpolysiloxane comprises between about 1/3 to 3/1.



INTERNATIONAL SEARCH REPORT

International Application No **PCT/US84/01068**

I. CLASSIFICATION OF SUBJECT MATTER (if several classification symbols apply, indicate all) ³

According to International Patent Classification (IPC) or to both National Classification and IPC ³

A 61L 15/06

U.S. CL 604,897

II. FIELDS SEARCHED

Minimum Documentation Searched ⁴

Classification System

Classification Symbols

U.S.

**604/304,307,896,897,344,128 DIG 21,640
523/111**

Documentation Searched other than Minimum Documentation
to the Extent that such Documents are Included in the Fields Searched ⁵

III. DOCUMENTS CONSIDERED TO BE RELEVANT ¹⁴

Category ⁶	Citation of Document, ¹⁵ with indication, where appropriate, of the relevant passages ¹⁷	Relevant to Claim No. ¹⁸
X	US, A, 3,598,122 August 10, 1971 ZAFFARONI	2
A	US, A, 2,857,356 October 21, 1958	1-10
A	US, A, 3,598,122 August 10, 1971	1,3-10
A	US, A 3,652,475 March 28, 1972	1-10
A	US, A, 4,039,707 August 02, 1977	1-10
A	US, A, 4,336,243 June 22, 1982	1-10
A	US, A, 4,016,328 April 05 1977	1-10
A	N, Noel, Chemistry and Technology of Silocones, pp. 386-389, Academic Press, 1968	1-10

⁶ Special categories of cited documents: ¹³

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier document but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"&" document member of the same patent family

IV. CERTIFICATION

Date of the Actual Completion of the International Search ¹

20 September 1984

Date of Mailing of this International Search Report ²

03 OCT 1984

International Searching Authority ¹

ISA/US

Signature of Authorized Officer ¹⁹

CHARLES ROSENBAUM
Charles Rosenbaum